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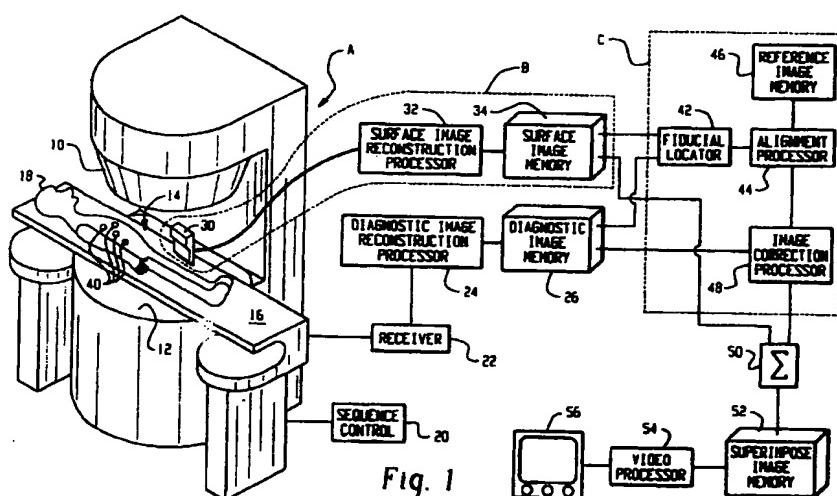
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### (54) External patient contouring

(57) An open MRI or other diagnostic imaging system (A) generates a three-dimensional diagnostic image representation, which is stored in an MRI image memory (26). A laser scanner or other surface imaging system (B) generates a volumetric surface image representation that is stored in a surface image memory (34). Typically, the volume and surface images are misaligned and the magnetic resonance image may have predictable distortions. An image correlating system (C)

determines offset, scaling, rotational, and non-linear corrections to the magnetic resonance image representation, which are implemented by an image correction processor (48). The corrected magnetic resonance image representation and the surface image representation are combined (50) and stored in a superimposed image memory (52). A video processor (54) generates image representations from selected portions of the superimposed image representation for display on a human-readable monitor (56).



**Description**

[0001] The present invention relates to the field of imaging. It finds particular application in conjunction with diagnostic imaging in open MRI scanners for oncology treatment applications and will be described with particular reference thereto. It will be appreciated, however, that the invention is also applicable to other types of diagnostic imaging for oncological purposes and for imaging for other purposes.

[0002] In oncological planning, the oncologist typically determines a point of entry on the patient's skin and a trajectory through the patient. Typically, the oncologist plans a trajectory and the point of entry in conjunction with projection x-ray images, CT scanner images, or other diagnostic images.

[0003] One of the difficulties encountered in oncological procedures is accurately aligning the x-ray beam with the internal tumor. If the selected trajectory is only slightly off, the x-ray beam will treat most of the tumor, but leave a small segment un-irradiated. Un-irradiated tumor tissue can survive the treatment.

[0004] Once the point of entry and the trajectory have been determined, the oncologist points an x-ray beam to enter the patient at the selected point of entry and follow the selected trajectory. Ideally, the x-ray beam is selected to have a diameter at least as large as the tumor to be irradiated. Making the diameter of the beam too large is detrimental in that it irradiates and harms healthy tissue.

[0005] Typically, the treatment process is repeated through a plurality of different trajectories to maximize the radiation at the tumor while minimizing radiation through surrounding tissue. In many instances, the tumor is over-irradiated to assure that portions of the tumor which might be missed along some trajectories are still fully irradiated. This over-radiation, like using a beam that is too large, has a detrimental effect on surrounding tissue.

[0006] Typically, x-ray images are used to generate the diagnostic images. X-ray images are advantageous in that they image the entire patient contour, including the surface boundaries facilitating selection of the point of entry. Unfortunately, it is sometimes difficult to differentiate between tissue types, such as cancerous and non-cancerous tissue with x-rays. Magnetic resonance imaging has much better differentiation of tissue types. However, magnetic resonance images tend to be of smaller, internal regions and often do not include the patient surface. When a larger region is imaged that includes the patient surface, peripheral portions of the image tend to be warped or distorted. Selecting the point of entry based on a warped or distorted image can cause mis-alignment between the beam and the cancerous tumor which, as discussed previously, can create the unwanted destruction of healthy tissue.

[0007] In accordance with one aspect of the present invention, a diagnostic imaging system is provided. A

medical diagnostic imaging apparatus generates volumetric diagnostic image representations of an internal region of a subject in an imaging region. A surface imaging system generates a three-dimensional image representation of the surface of the subject in the imaging region. An image correlating system correlates the surface and diagnostic image representations. A superimposed volumetric image representation memory stores combined correlated surface and diagnostic image representations. A video processor withdraws selected portions of the combined image representation and converts them into appropriate form for human-readable display.

[0008] In accordance with another aspect of the present invention, a method of diagnostic imaging is provided. A volumetric diagnostic image representation of an internal region of a subject and at least a portion of a surface of the subject is generated. However, the diagnostic image representation has distortions, particularly in a region adjacent the surface of the subject. A surface imaging system generates a three-dimensional image representation of the surface of the subject. The diagnostic image representation is adjusted to correlate at least the surface region of the diagnostic image representation with the surface image representation. The adjusted diagnostic image representation and the surface image representation are combined.

[0009] One advantage of the present invention is that it permits improved differentiation of soft tissue.

[0010] Another advantage of the present invention is that it facilitates a reduction in radiation doses in oncological treatments.

[0011] Another advantage of the present invention is that it facilitates location of internal patient structures from the exterior of the patient based on diagnostic images.

[0012] Another advantage of the present invention is that it reduces total patient radiation dose relative to x-ray and CT diagnostic imaging techniques.

[0013] One way of carrying out the invention will now be described in detail, by way of example, with reference to the accompanying drawing (Figure 1), which is a diagrammatic illustration of an image generation system in accordance with the present invention.

[0014] With reference to FIGURE 1, a medical diagnostic imaging apparatus A, such as an open magnetic resonance imaging system, generates a volumetric image of an internal region of the patient including a portion of the patient surface. A surface imaging system B generates a volumetric image of the patient surface. An imaging correlating system C scales, shifts, rotates, and non-linearly adjusts the medical diagnostic image to bring it into correlation with the surface image representation. The correlated images are combined to provide a combined or superimposed image of interior and surface from which the oncologist extracts medically appropriate slice, 3D rendered, or other images for planning the oncological procedure.

[0015] The diagnostic imager **A** in the preferred embodiment is a vertical field magnetic resonance imaging system that includes an upper pole 10 and a lower pole 12. Magnets, preferably superconducting, generate a vertical magnetic field through an imaging region 14 between the poles 10 and 12. A patient support 16 is movable in three dimensions to position a region of interest of a subject 18 in the imaging region.

[0016] A sequence control processor 20 controls gradient and radio frequency coils associated with the poles 10, 12 of the magnetic resonance imager to induce and manipulate magnetic resonance, as is known in the art, to generate magnetic resonance signals. The generated magnetic resonance signals are picked by radio frequency coils, demodulated by a receiver 22, and reconstructed by an MRI image reconstruction processor 24 into an electronic image representation. The electronic image representation of the region of interest of the subject disposed in the imaging region 14 is stored in an MRI volume image memory 26.

[0017] The surface imaging system **B** in the preferred embodiment is a hand-held laser scanning system. More specifically, the laser scanning system includes a hand-held unit 30 which sweeps a laser beam. The hand-held unit 30 is positioned such that the laser beam scans the surface of the subject 18 in the imaging region 14. The reflected laser light received by the hand-held unit 30 generates electronic signals which are conveyed to a surface image reconstruction processor 32 which reconstructs an electronic image representation of the surface of the subject 18 in three dimensions. A surface volume image memory 34 stores the electronic image representation. Other known surface imaging systems are also contemplated, such as ultrasonic imaging systems, optical imaging systems such as those with stereo cameras, mechanical arms which are moved over the surface, and the like.

[0018] In order to facilitate coordination of the surface and MRI diagnostic images, a plurality of fiducials 40 that are imageable by both the MRI imaging system and the surface imaging system, are preferably adhered to several, scattered positions on the surface of the patient in the examination region. Alternately, anatomical markers that are identifiable in both images can be utilized analogously. The image correlating system **C** includes a fiducial locating processor 42 which examines the electronic surface and diagnostic image representations to identify the fiducials 40 in each. More specifically, the fiducial locating processor 42 generates a three-dimensional image representation of the fiducials 40 in the diagnostic image. An alignment processor 44 compares the position of the fiducials in the two images. In one embodiment, the alignment processor 44 determines the baricenter of the fiducials 40 in each of the aforementioned images and determines an offset or linear shift therebetween. The alignment processor also determines the distance between the baricenter and each of the fiducials 40 in each of the aforementioned

images and determines a scaling factor in accordance with the variation therebetween. The alignment processor 44 also determines rays between the baricenter and the fiducials 40 in each of the aforementioned images and determines an angular offset or rotational correction between the two. Preferably, the alignment processor 44 also accesses a reference image from a reference image memory 46 to perform higher order alignment functions. More specifically to the preferred embodiment,

5 an image of a phantom is generated with the medical diagnostic imaging apparatus **A**. Based on differences between the known shape of the phantom and the shape of the image, non-linear distortion adjustments for the diagnostic imaging apparatus **A** are generated and stored in the reference image memory 46.

10 [0019] The offset, scaling, rotational, and non-linear image corrections determined by the alignment processor 44 are conveyed to an image correction processor 48 which operates on the medical diagnostic image representation to bring it into alignment with the surface image representation.

15 [0020] The surface and corrected diagnostic image representations are combined 50 and stored in a superimposed volumetric image memory 52. Under control of the oncologist, a video processor 54 selects portions of the superimposed volumetric image representation from the superimposed image memory 50 and converts them into appropriate form and format for display on a monitor 56 such as a video monitor, CCD display, active matrix, or the like. The video processor 52 may select slice images, surface renderings, projection images, or other diagnostic imaging formats as are known in the art.

20 [0021] In an alternate embodiment, the image alignment system uses a calibration phantom scan. A phantom, such as one with a three-dimensional grid of fiducials, is imaged with the MRI system. The fiducial locator 42 locates the fiducials in the MRI image representation. The alignment processor compares the actual fiducial positions with the imaged positions and generates correction factors. The correction factors can be as discussed above, vector shifts for each of a plurality of subregions, or the like. The correction factors are loaded into the image correction processor 48. Optionally, a similar correction factor determining procedure is performed with the surface imaging system and loaded into an analogous image correction processor for the surface volume image. When a patient is subsequently imaged, the MRI image representation and, optionally, the surface image representation, are corrected as generated with the preloaded corrections without fiducials on the patient or the on-the-fly fiducial correlation processing.

25 [0022] The image alignment system can also be used to align the MRI image representation with the surface image representation. The alignment processor 44 compares the positions of the fiducials 40 in the MRI image representation with the positions of the fiducials 40 in the surface image representation. The alignment processor 44 generates correction factors for the MRI image representation based on the comparison. The correction factors are loaded into the image correction processor 48. The image correction processor 48 corrects the MRI image representation based on the correction factors. The corrected MRI image representation is then combined with the surface image representation to produce a superimposed volumetric image memory 52.

30 [0023] The image alignment system can also be used to align the surface image representation with the MRI image representation. The alignment processor 44 compares the positions of the fiducials 40 in the surface image representation with the positions of the fiducials 40 in the MRI image representation. The alignment processor 44 generates correction factors for the surface image representation based on the comparison. The correction factors are loaded into the image correction processor 48. The image correction processor 48 corrects the surface image representation based on the correction factors. The corrected surface image representation is then combined with the MRI image representation to produce a superimposed volumetric image memory 52.

35 [0024] The image alignment system can also be used to align the MRI image representation with the surface image representation. The alignment processor 44 compares the positions of the fiducials 40 in the MRI image representation with the positions of the fiducials 40 in the surface image representation. The alignment processor 44 generates correction factors for the MRI image representation based on the comparison. The correction factors are loaded into the image correction processor 48. The image correction processor 48 corrects the MRI image representation based on the correction factors. The corrected MRI image representation is then combined with the surface image representation to produce a superimposed volumetric image memory 52.

40 [0025] The image alignment system can also be used to align the surface image representation with the MRI image representation. The alignment processor 44 compares the positions of the fiducials 40 in the surface image representation with the positions of the fiducials 40 in the MRI image representation. The alignment processor 44 generates correction factors for the surface image representation based on the comparison. The correction factors are loaded into the image correction processor 48. The image correction processor 48 corrects the surface image representation based on the correction factors. The corrected surface image representation is then combined with the MRI image representation to produce a superimposed volumetric image memory 52.

45 [0026] The image alignment system can also be used to align the MRI image representation with the surface image representation. The alignment processor 44 compares the positions of the fiducials 40 in the MRI image representation with the positions of the fiducials 40 in the surface image representation. The alignment processor 44 generates correction factors for the MRI image representation based on the comparison. The correction factors are loaded into the image correction processor 48. The image correction processor 48 corrects the MRI image representation based on the correction factors. The corrected MRI image representation is then combined with the surface image representation to produce a superimposed volumetric image memory 52.

50 [0027] The image alignment system can also be used to align the surface image representation with the MRI image representation. The alignment processor 44 compares the positions of the fiducials 40 in the surface image representation with the positions of the fiducials 40 in the MRI image representation. The alignment processor 44 generates correction factors for the surface image representation based on the comparison. The correction factors are loaded into the image correction processor 48. The image correction processor 48 corrects the surface image representation based on the correction factors. The corrected surface image representation is then combined with the MRI image representation to produce a superimposed volumetric image memory 52.

55 [0028] The image alignment system can also be used to align the MRI image representation with the surface image representation. The alignment processor 44 compares the positions of the fiducials 40 in the MRI image representation with the positions of the fiducials 40 in the surface image representation. The alignment processor 44 generates correction factors for the MRI image representation based on the comparison. The correction factors are loaded into the image correction processor 48. The image correction processor 48 corrects the MRI image representation based on the correction factors. The corrected MRI image representation is then combined with the surface image representation to produce a superimposed volumetric image memory 52.

60 [0029] The image alignment system can also be used to align the surface image representation with the MRI image representation. The alignment processor 44 compares the positions of the fiducials 40 in the surface image representation with the positions of the fiducials 40 in the MRI image representation. The alignment processor 44 generates correction factors for the surface image representation based on the comparison. The correction factors are loaded into the image correction processor 48. The image correction processor 48 corrects the surface image representation based on the correction factors. The corrected surface image representation is then combined with the MRI image representation to produce a superimposed volumetric image memory 52.

65 [0030] The image alignment system can also be used to align the MRI image representation with the surface image representation. The alignment processor 44 compares the positions of the fiducials 40 in the MRI image representation with the positions of the fiducials 40 in the surface image representation. The alignment processor 44 generates correction factors for the MRI image representation based on the comparison. The correction factors are loaded into the image correction processor 48. The image correction processor 48 corrects the MRI image representation based on the correction factors. The corrected MRI image representation is then combined with the surface image representation to produce a superimposed volumetric image memory 52.

70 [0031] The image alignment system can also be used to align the surface image representation with the MRI image representation. The alignment processor 44 compares the positions of the fiducials 40 in the surface image representation with the positions of the fiducials 40 in the MRI image representation. The alignment processor 44 generates correction factors for the surface image representation based on the comparison. The correction factors are loaded into the image correction processor 48. The image correction processor 48 corrects the surface image representation based on the correction factors. The corrected surface image representation is then combined with the MRI image representation to produce a superimposed volumetric image memory 52.

75 [0032] The image alignment system can also be used to align the MRI image representation with the surface image representation. The alignment processor 44 compares the positions of the fiducials 40 in the MRI image representation with the positions of the fiducials 40 in the surface image representation. The alignment processor 44 generates correction factors for the MRI image representation based on the comparison. The correction factors are loaded into the image correction processor 48. The image correction processor 48 corrects the MRI image representation based on the correction factors. The corrected MRI image representation is then combined with the surface image representation to produce a superimposed volumetric image memory 52.

## 55 Claims

- An imaging system comprising: an imaging apparatus (**A**) for generating volumetric image representations;

- tations of an internal region of a subject (18) in an imaging region (14); a surface imaging system (B) for generating a three-dimensional image representation of a surface of the subject in the imaging region; an image correlating system (C) for correlating the surface and volumetric image representations; a superimposed volumetric image representation memory (52) for storing the combined, correlated surface and volumetric image representations; and a video processor (54) for withdrawing selected portions of the combined image representation, and converting them into appropriate form for human-readable display.
2. An imaging system as claimed in claim 1, further including a plurality of fiducials (40) disposed in the imaging region (14), the fiducials being arranged to be imaged by both the imaging apparatus (A) and the surface imaging system (B) such that images of the fiducials appear in both the surface image representation and the volumetric image representation and wherein the image correlating system includes: a fiducial locating processor (42) for determining a location of the fiducials in each of the surface and volumetric image representations; and an alignment processor (44) for comparing the locations of the fiducials determined by the fiducial locating processor (42) to determine a spatial deviation between the surface and volumetric image representations.
3. An imaging system as claimed in claim 2, further including: an image correction processor (48) connected with the alignment processor to correct at least one of the volumetric and surface image representations in accordance with the determined deviation between the images.
4. An imaging system as claimed in claim 2 or claim 3, wherein the alignment processor (44) further accesses a reference memory (46) which stores information indicative of non-linear distortion in the at least one of the volumetric and surface image representations and determines a non-linear image adjustment in accordance therewith.
5. A method of imaging comprising: generating a volumetric image representation of an internal region of a subject including at least a portion of a surface of the subject, which volumetric image representation is distorted in a region adjacent the subject surface; generating a surface image representation of the surface of the subject; adjusting at least the surface region of the volumetric image representation in accordance with the surface image representation; combining the surface image representation and the adjusted volumetric image representation.
6. A method as claimed in claim 5, further including: prior to generating the volumetric image representation, generating a phantom image representation of a phantom; comparing the phantom image with physical dimensions of the phantom; determining and storing correction factors in accordance with a difference between the phantom image representation and the dimensions of the phantom; the adjusting step including adjusting the volumetric image representation in accordance with the stored correction factors.
7. A method as claimed in claim 6, further including: identifying a plurality of characteristic points on the subject surface; identifying the characteristic points in the volumetric image representation and the surface image representation; and wherein the adjusting step includes: determining a variation between the locations of the characteristic points in the volumetric image representation and the surface image representation, and adjusting the volumetric image representation in accordance with both the variations and the stored correction factors.
8. A method as claimed in claim 7, further including: affixing fiducials (40) which are identifiable in both the volumetric image representation and the surface image representation to the characteristic points on the subject surface.
9. A method as claimed in claim 7 or claim 8, wherein the step of determining the variation includes: determining an offset, a scaling factor, and a rotation between the locations of the characteristic points in the volumetric and surface image representations.
10. A method of imaging as claimed in any one of claims 5 to 9, wherein the step of generating the surface image representation includes one of laser scanning, video scanning, and ultrasonic scanning of the surface of the subject.

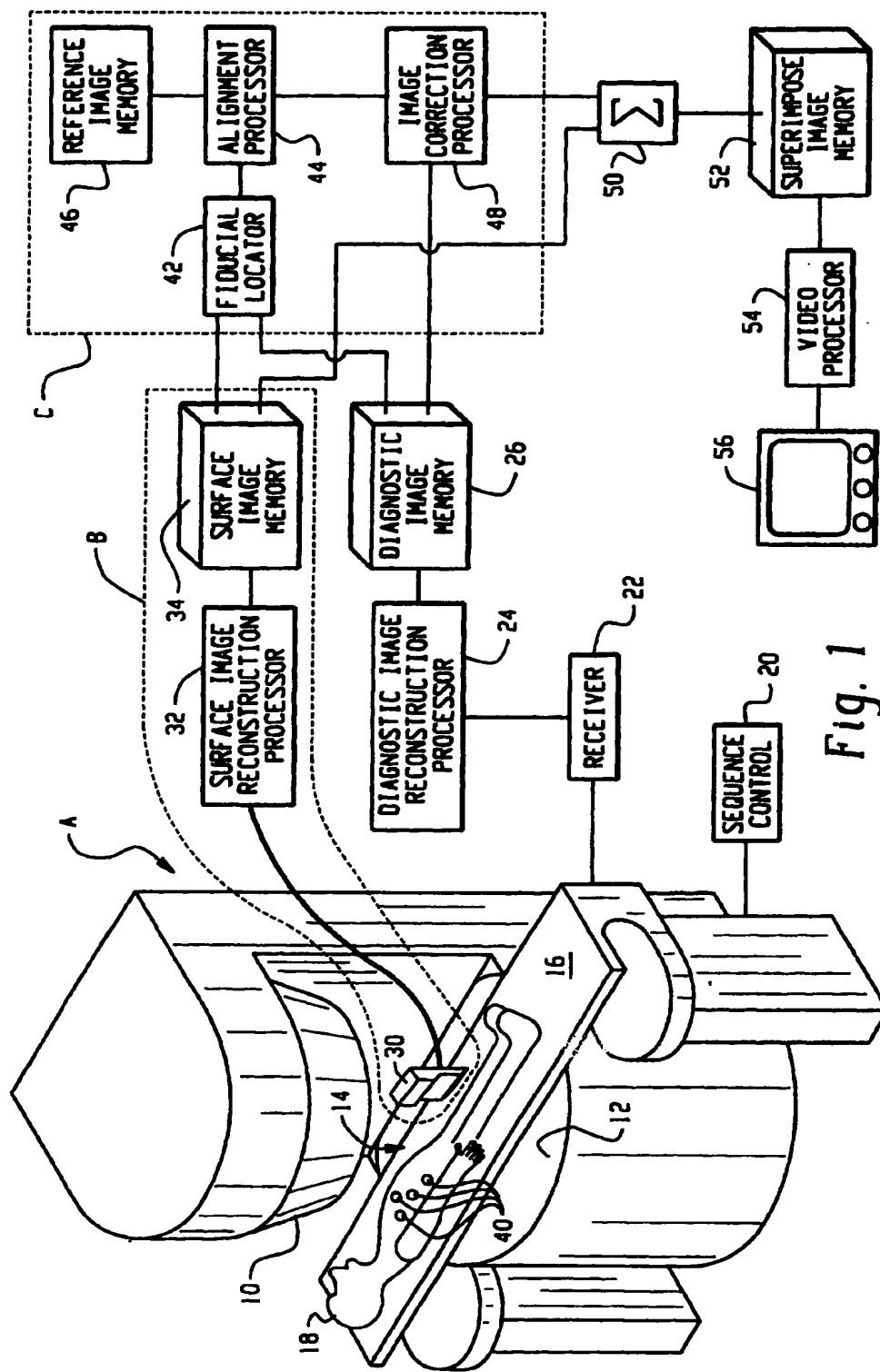


Fig. 1